Center for Wearable Sensors



Wearable Chemical Sensors: Opportunities and Challenges

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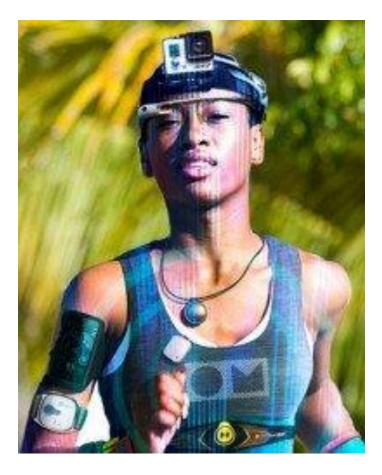
UC San Diego

Wearables: an exciting high-growth market



UCSD

Why aren't we there now?



Size & Usability:

Need to develop sensors that are small & seamlessly integrated into daily life

Battery Life:

Need ultra-low-power and/or energy harvesting to minimize re-charging

Utility:

Need to develop sensors that are <u>actually useful</u>

Wearable sensing opportunities

Physical attributes

- Motion (e.g., steps)
- Temperature
- Respiration
- Blood pressure

Electrical attributes

- ECG (heart)
- EEG (brain)
- EMG (muscles)

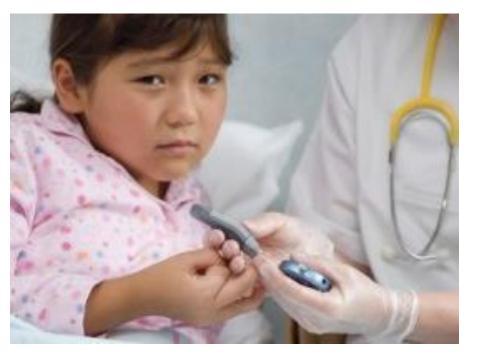
Most of the wearables market today

Biochemical attributes

- Glucose
- Electrolytes
- Alcohol
- Lactate
- Many more!

Opportunity!

Chemical analysis: current practice



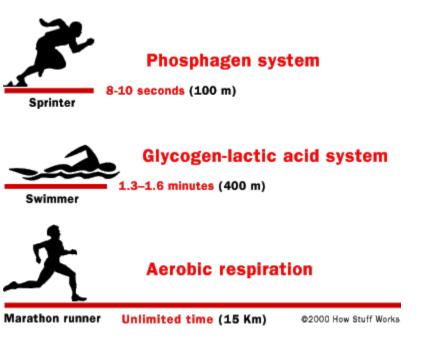


Painful / inconvenient blood draws



Example: lactate monitoring for athletes

Staying below the "lactate threshold" important for endurance training





Current state-of-the-art testing method:



Non-invasive and/or continuous sensing is required



Non-Invasive Chemical Biosensing Techniques

Bioimpedance Spectroscopy

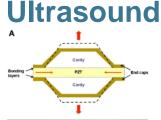
Adamson et. al. Analyst 2012

mm-wave Detection





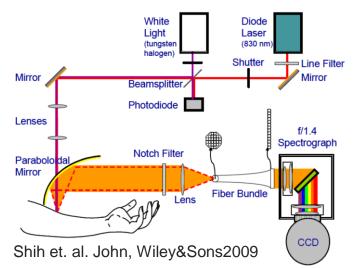
Jean et. al. SAS IEEE 2008



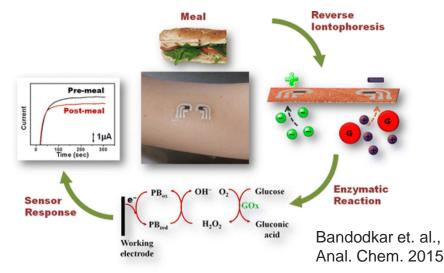


Park et. al. J Diabetes Sci Technol, 2009

Raman Spectroscopy



Electrochemical



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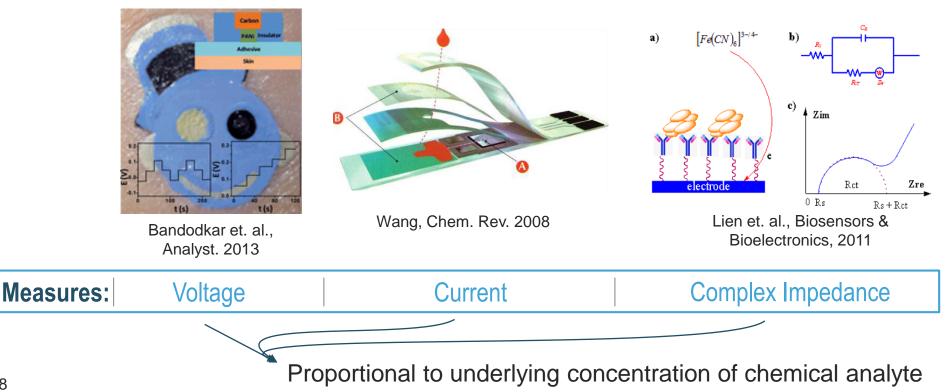
Electrochemical Biosensors

Chemical communicate via ions, electronics via electrons. Electrochemical biosensors operate by measuring electrons as the output of redox reactions. Three main types of sensors:

Potentiometric

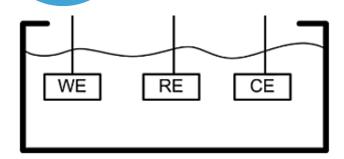
Amperometric

Electrochemical Impedance Spectroscopy (EIS)



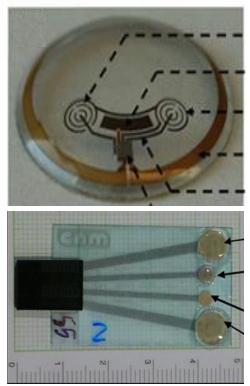


Biosensor Fabrication



Most electrochemical biosensors rely on two- or threeelectrode systems: a working electrode (WE), a reference electrode (RE), and sometimes a counter electrode (CE). Electrodes are functionalized for analyte specificity, and can be fabricated on many different materials:

Plastics



Textiles





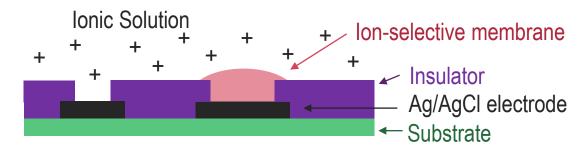
Temporary Tattoos





Instrumentation Circuits: Potentiometric Biosensors

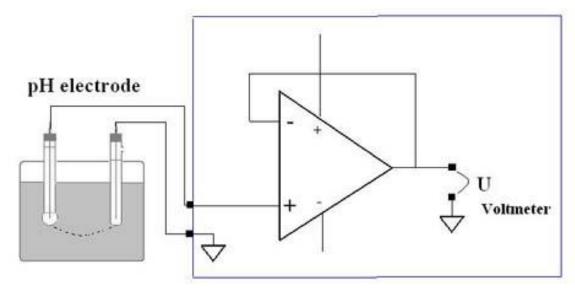
Example: measure the voltage between a reference electrode and an electrode with an ionselective membrane coating



Applications: pH, K⁺, Na^{+,} Cl⁻, etc...

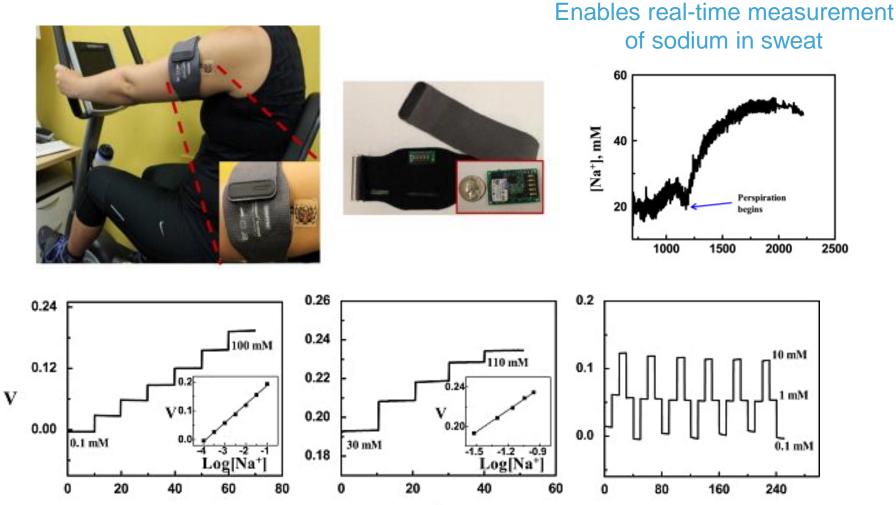
Typical Instrumentation Amplifier Requirements:

Voltage range: 0-400mV
Noise: several µV
Bandwidth: < 100Hz





Example: a wearable sodium sensor tattoo



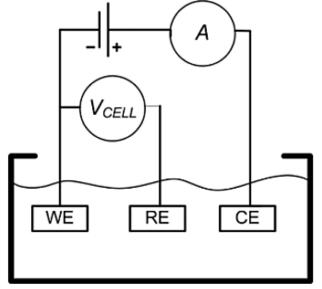
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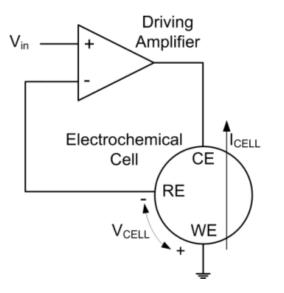
Bandodkar et al., Biosensors & Bioelectronics, 2014.

Amperometric biosensors: sensing metabolites

Selectivity: working electrode functionalized with an enzyme that catalyzes a reaction with the metabolite to be sensed, which then transfers e⁻ to an ISE underneath

Operating principal: enzymatic reaction occurs at specific voltage \rightarrow apply voltage, measure resulting current \rightarrow proportional to analyte concentration



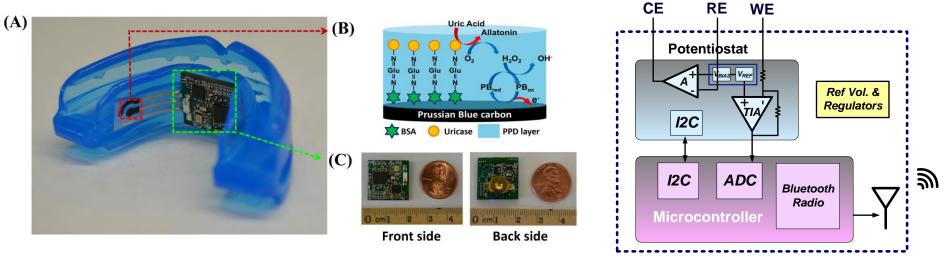


Circuit: potentiostat used to condition the cell; current sensor (e.g., TIA) to sense current, often through the counter electrode to not disturb cell potential

Typical Requirements:

- □ Voltage range: ±1∨
- **Current range:** fA µA
- ❑ Noise: lower current range
- **Amp. voltage gain:** > 10^4

Example System: A Saliva-Sensing Mouthguard (1)



J. Kim et al., Biosensors & Bioelectronics, 2015

Fitness applications

Measure Lactate for Stress / Exertion



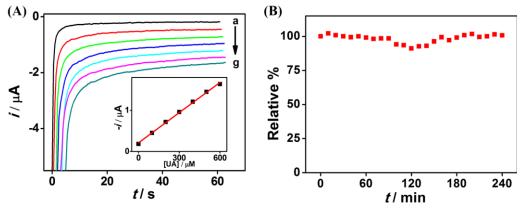
Health applications

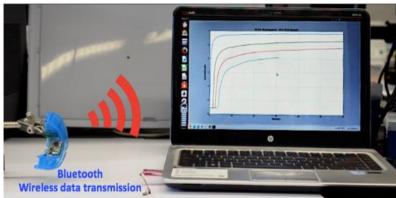
Measures Uric Acid for Hyperuricemia



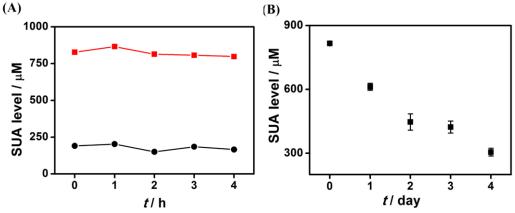
Example System: A Saliva-Sensing Mouthguard (2)

Characterization of integrated wireless mouthguard biosensor



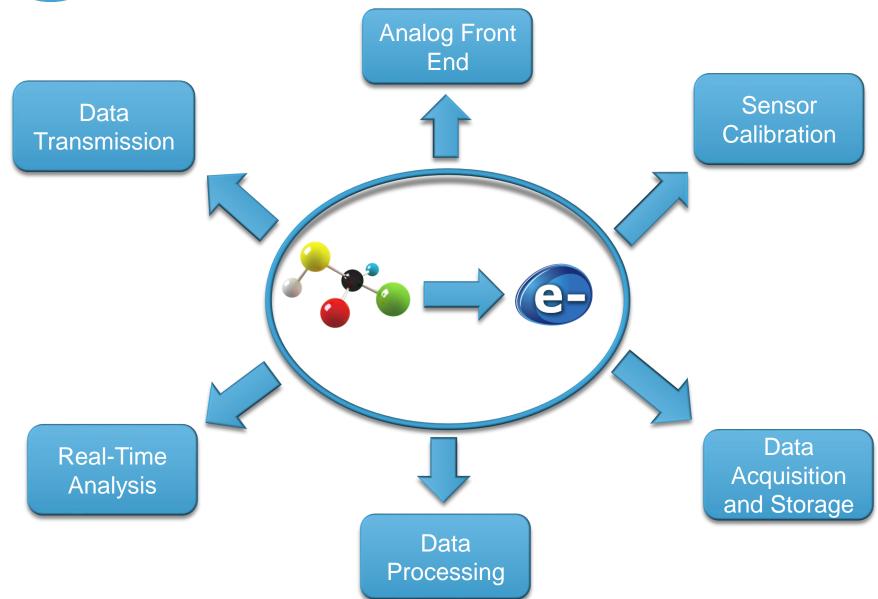


Monitoring treatment of hyperuricemia with Allopurinol®





Chemical biosensing system considerations



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Challenge: Efficient Calibration for Operation in Complex Fluids

Selectivity: ISEs are not perfectly selective → other ions in solution will affected measured potential

UCSI

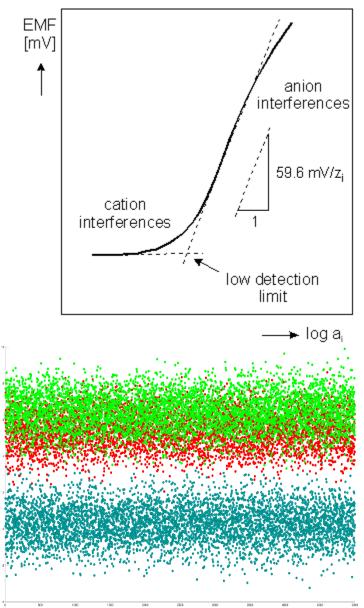
$$V = V_0 + \frac{RT}{z_i F} \ln \left(a_i + \sum_j \frac{k_{ij} a_j^{\frac{Z_i}{Z_j}}}{n} \right)$$

Finite selectivity coefficients

Challenge: may require significant calibration with many analytes to represent real (complex) fluids

Opportunity: leverage machine-learning to quickly infer selectivity coefficients

Location: calibrate and/or process ondevice, in the fog, or in the cloud

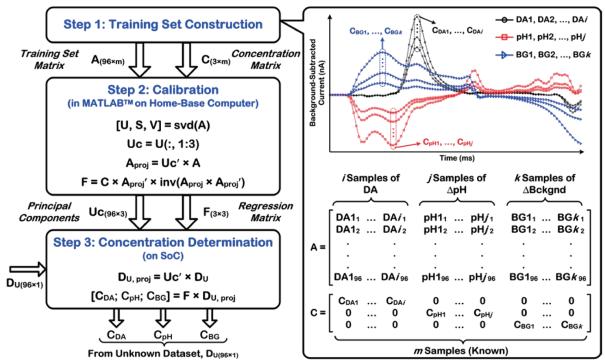




Example: dopamine monitoring in complex fluids

Challenge: dopamine sensors vary with pH and background interferers

Solution: in-sensor principal component regression (PCR)-based chemometrics to infer dopamine concentration



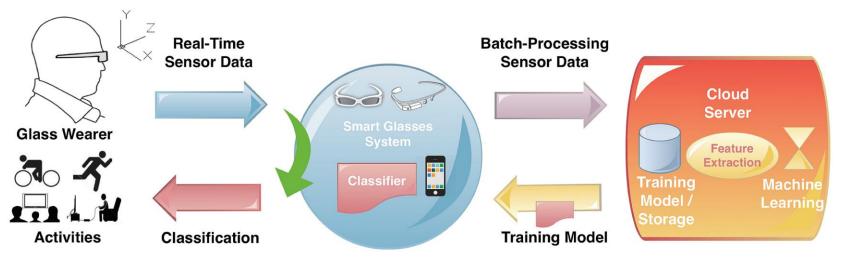
Bozorgzadeh et. al., VLSI, 2015

Leverage multi-variate analysis to improve specificity in complex environments



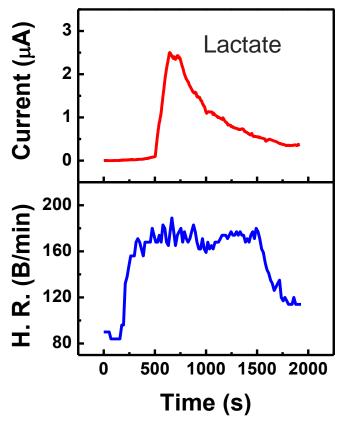
 Real-time chemical data is generally not available today. We don't know what kind of correlations to expect – analytics will help

Example: classifying user's head motions to recognize activities according to wearable sensor data from the smart glasses

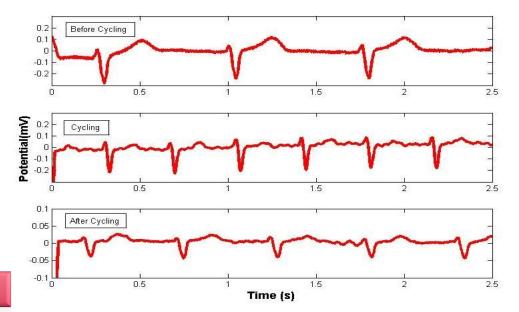


Ho and Wang, User-Centric and Real-Time Activity Recognition Using Smart Glasses, 2015

Simultaneous & continuous, real-time lactate and ECG sensing







S. Imani et al., Nature Communications, May 2016

First demonstration of simultaneous chemical+electrophysiological sensing in a wearable patch

Opportunities for data analytics



- Current wearable sensors have limited utility
- Introduction of chemical sensing can augment utility across a number of applications spaces:
 - High-end athletes
 - Diabetic patients
 - General-purpose "tricorder-like" monitoring
- There are many challenges:
 - Sensor fabrication on soft wearable materials
 - Miniaturized, low-power electronics
 - Low-cost calibration
 - Interference & longevity
 - Analytics & inference

Can be solved with big-data analytics & machine learning

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